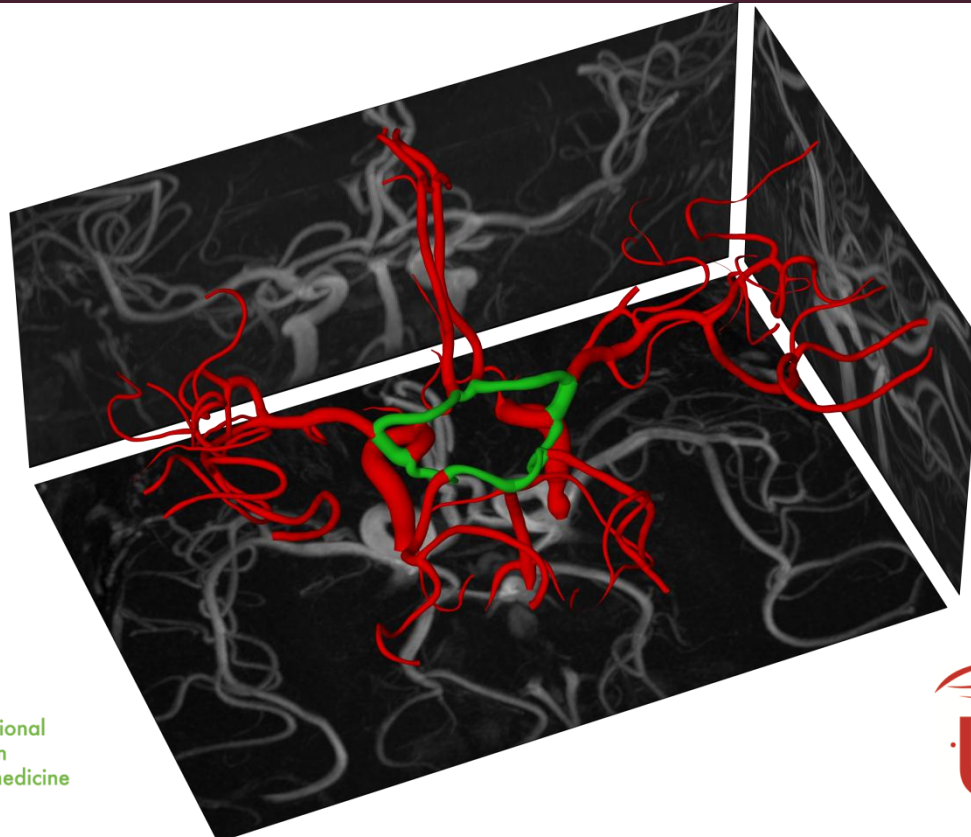


Geometric Modeling and Characterization of the Circle of Willis

Hrvoje Bogunović

CCVW 2012 / Zagreb, Croatia / 2012-09-21



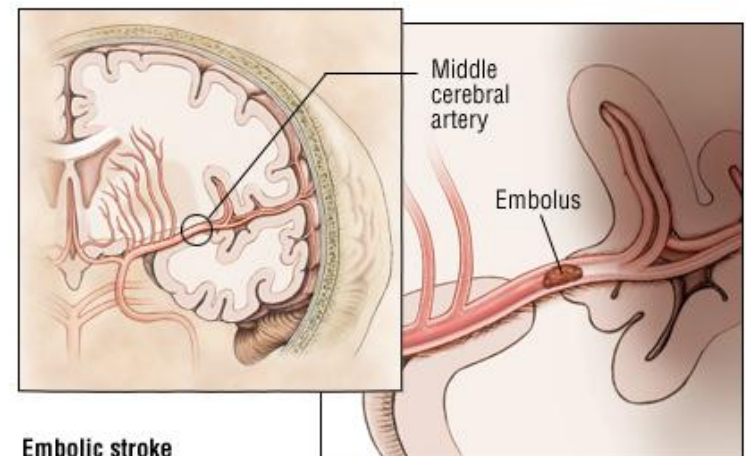
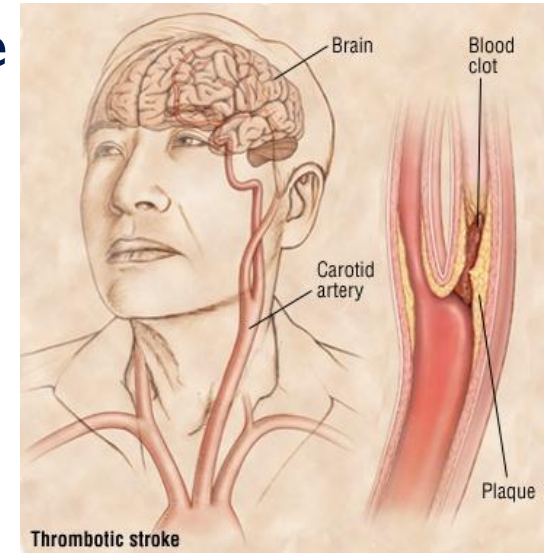
- Brain depends critically on its blood supply
 - 15% of cardiac output
- Cerebrovascular disease can lead to a stroke
 - Atherosclerosis
 - Aneurysms
- Stroke
 - Major cause of disability
 - Second leading cause of death
 - Western society
 - Ischemic (80%)
 - Thrombotic, embolic
 - Hemorrhagic (20%)



Saccular Aneurysm

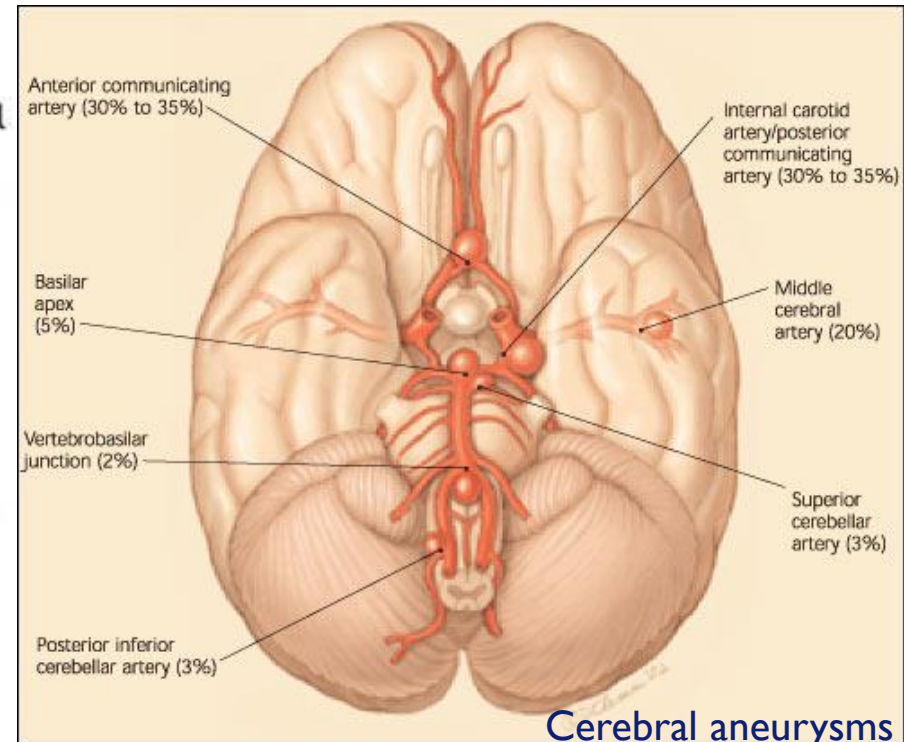
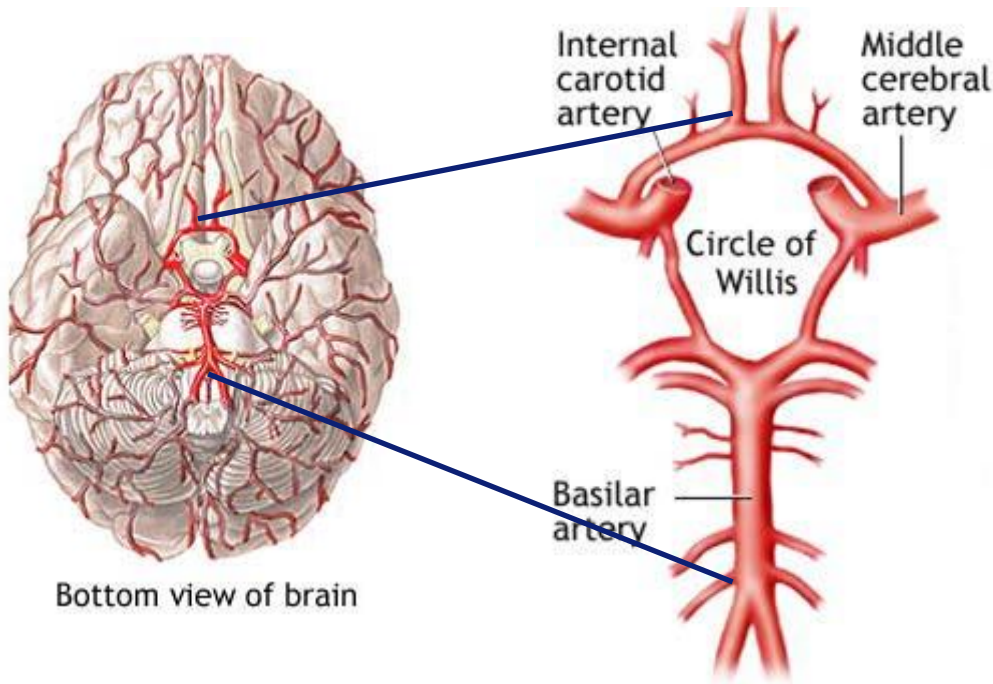
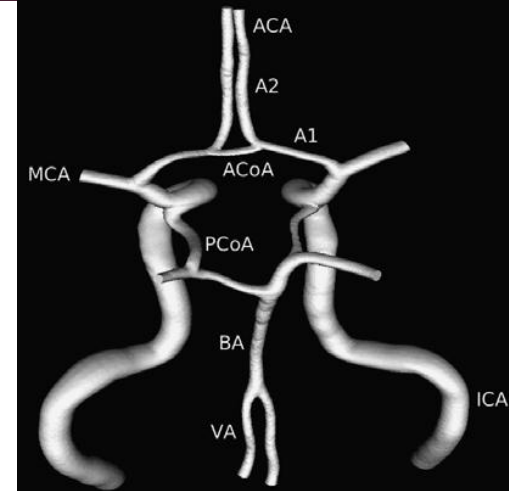


Ruptured Aneurysm



■ Focus on the Circle of Willis

- Conducts the blood flow from the anterior-left, anterior-right and posterior circulation to the brain
- Arterial system forms a cycle by design
- Common site of pathologies
- Large anatomical variability



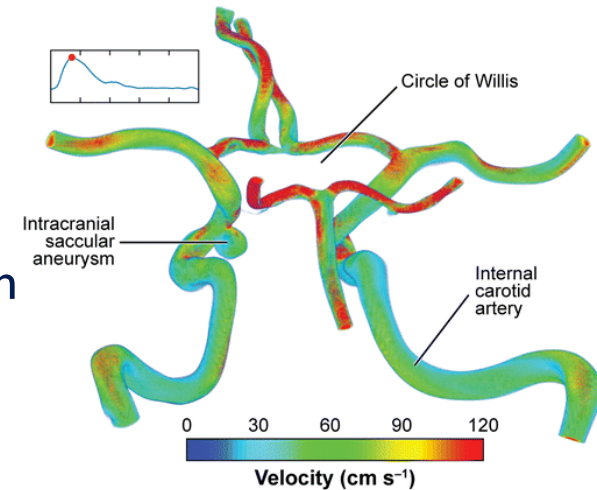
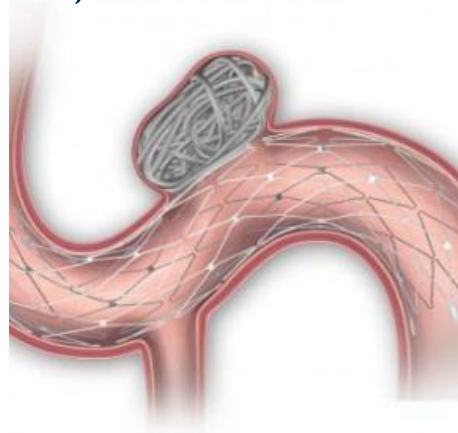
■ Geometric risk factors*


- Cerebral aneurysms occur at specific locations, at or near high curvature
- Atherosclerosis often occurs at carotid bifurcation or close to arterial bendings
- Hypothesis: hemodynamics responsible
 - Dependent on geometry

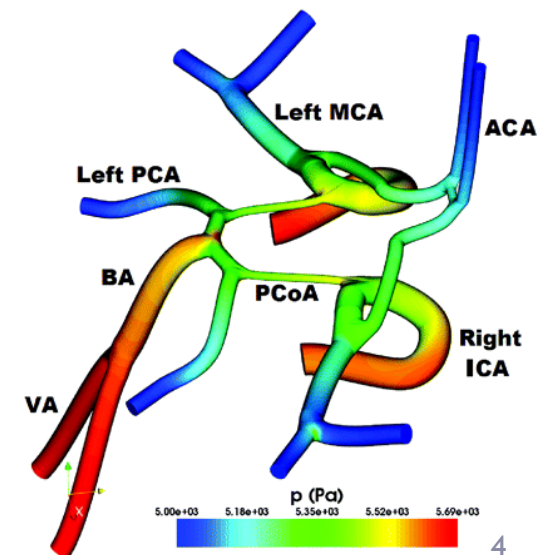
* Friedman et al., Atherosclerosis, vol. 46, pp. 225–231, Feb. 1983.

■ Endovascular treatment difficulty

- Device selection, and intervention planning
- Stent fitness

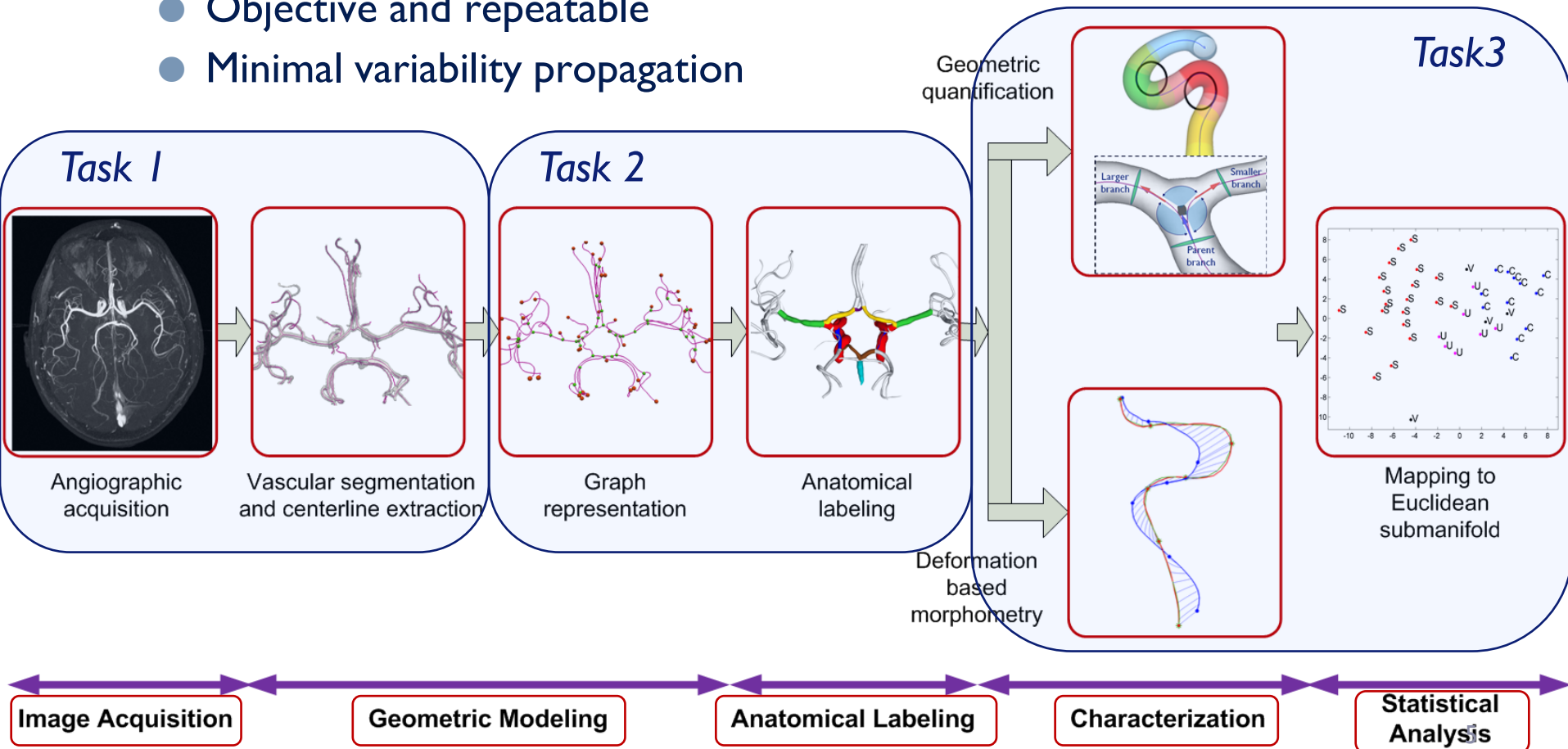


 Humphrey JD, Taylor CA. 2008. Annu. Rev. Biomed. Eng. 10:221–46.

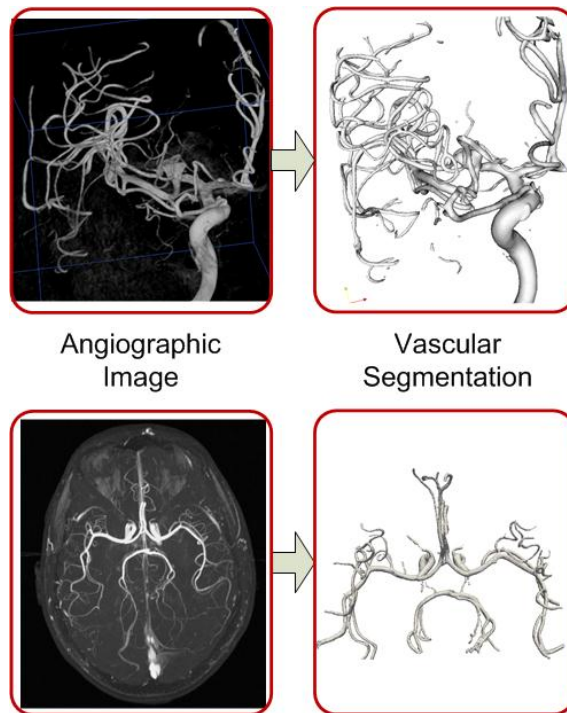


Alnaes et al., Stroke, 2007.

- Processing pipeline for image-based, subject-specific geometry characterization of the Circle of Willis
- High level of automation
 - Objective and repeatable
 - Minimal variability propagation

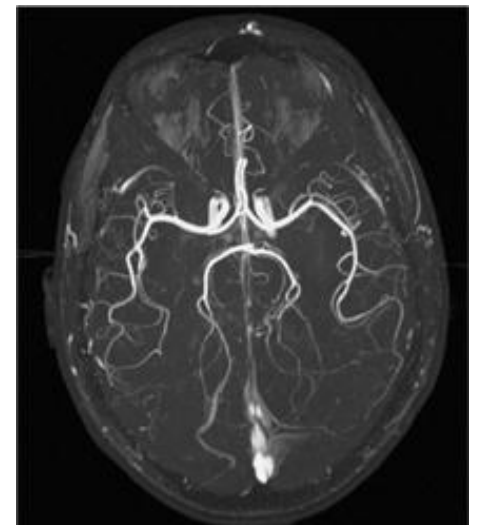
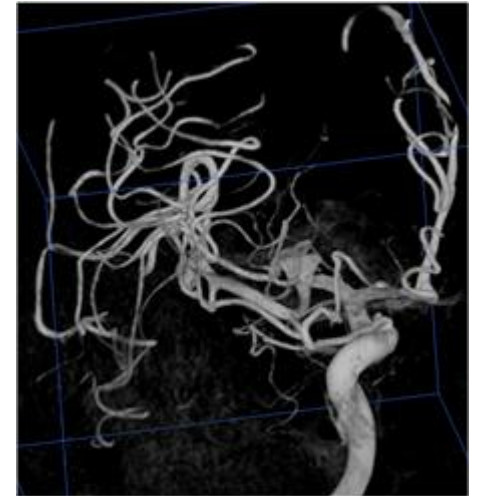


TI: SEGMENTATION OF CEREBRAL VASCULATURE



H. Bogunović, J.M. Pozo, M.C. Villa-Uriol, C.B.L.M. Majoie, R. Van Den Berg, H.A.F. Gratama Van Andel, J.M. Macho, J. Blasco, L. San Román, A.F. Frangi: Automated segmentation of cerebral vasculature with aneurysms in 3DRA and TOF-MRA using geodesic active regions: an evaluation study. *Medical Physics*, vol. 38(1), Jan. 2011, pp. 210-222.

- Objective: From angiographic image obtain accurate geometric model of vasculature containing pathologies (aneurysms)
 - Focus on 3DRA and MRA imaging modalities
- 3DRA
 - Invasive: contrast injected into artery + radiation
 - Treatment planning and evaluation
 - High image spatial resolution ($0.2 \times 0.2 \times 0.2 \text{ mm}^3$)
- ToF-MRA
 - Non-invasive, no contrast, no radiation
 - Screening and follow-up. Volunteers.
 - Anisotropic spatial resolution ($0.5 \times 0.5 \times 0.8 \text{ mm}^3$)
 - Full CoW observed



Geodesic Active Regions (GAR)

- Geometric deformable model using the level set framework
 - Completely automated (including initialization)

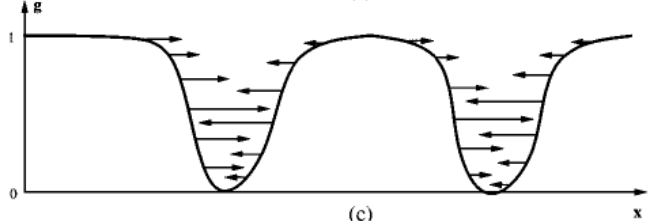
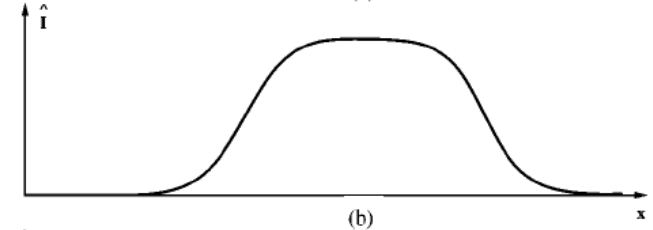
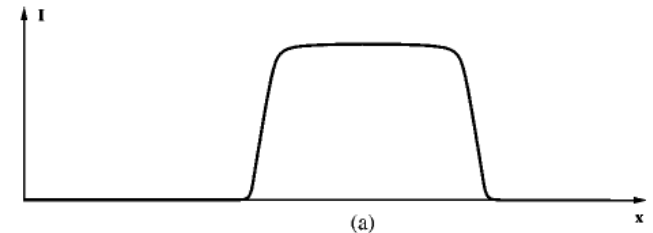
$\Psi(x, t)$									
		-2.4	-1.3	-0.6	-0.7	-0.8	-1.8		
	-2.4	-1.4	-0.3	0.4	0.3	0.2	-0.8	-1.8	
-2.4	-1.4	-0.4	0.6	1.6	1.3	1.2	0.3	-0.8	-1.8
-1.2	-0.2	0.8	1.8			2.3	1.3	0.3	-0.7
-1.1	-0.1	0.9	0.7	1.7		1.2	0.2	-0.8	
-2.5	-1.5	-0.5	-0.3	0.7	2.4	1.4	0.4	-0.6	
-2.5	-1.5	-1.3	-0.4	1.3	0.3	0.4	-0.6		
		-1.6	-0.6	0.4	-0.7	-0.6	-1.6		
		-1.6	-0.6	-1.7					

$$\frac{\partial}{\partial t} \Phi + \zeta \left(\overset{\text{region}}{k_{out} - k_{in}} \right) | \nabla \Phi | - \eta \left(\overset{\text{curvature}}{\varepsilon g K_m} \right) | \nabla \Phi | + \overset{\text{gradient}}{\nabla g \cdot \nabla \Phi} = 0$$

- Gradient term:
 - From geodesic active contour (GAC)
 - Surface at local gradient maximum (objective)

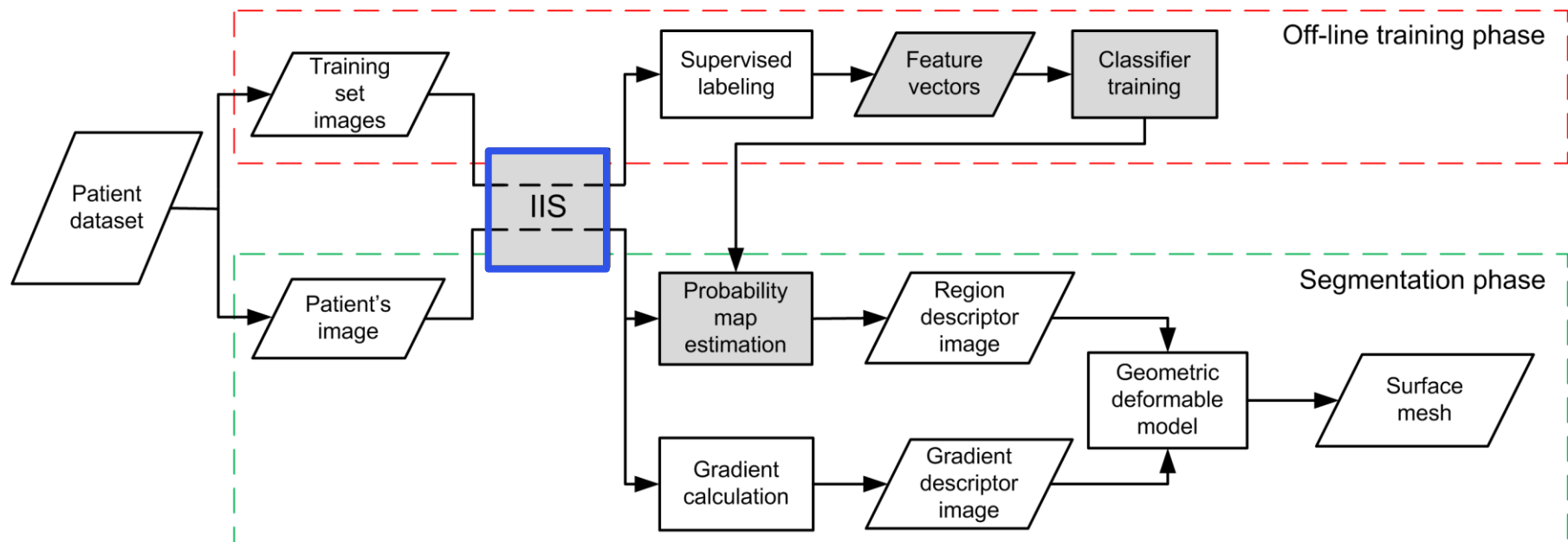
$$g = \frac{1}{1 + |\nabla \hat{I}|^p}$$

- Region term: use of training-set
 - Learns vessel and background features
 - Differential invariants (multiscale)
 - Intensity
 - Gradient magnitude, Laplacian ...



GAR workflow

- 3DRA and MRA: No correspondence tissue-intensity
- Introduction of the image intensity standardization (IIS)



M. Hernandez and A. F. Frangi, *Medical Image Analysis*, 2007.

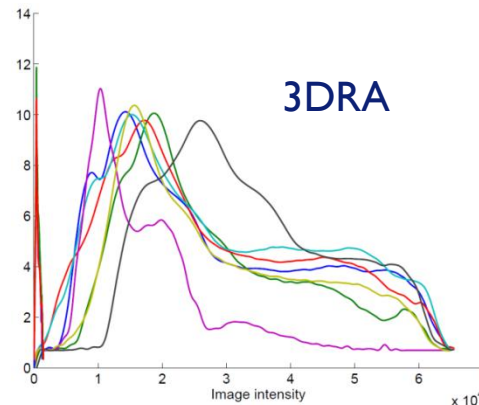
H. Bogunović, et al., *SPIE Medical Imaging*, 2008.

H. Bogunović et al, *Medical Physics*, 2011.

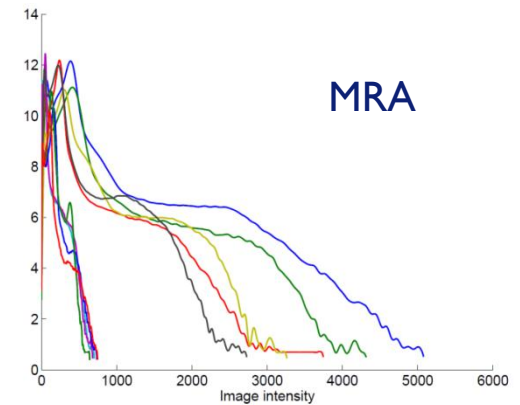
GAR - Image Intensity Standardization (IIS)

■ Non-linear signal registration to a histogram reference

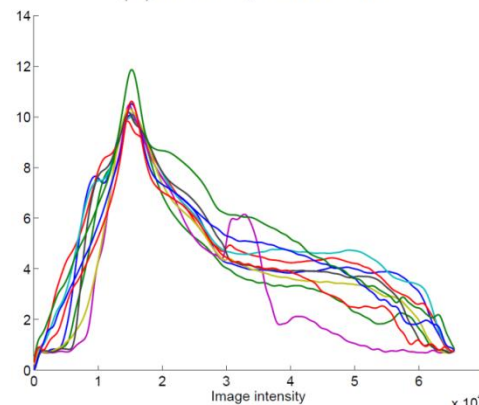
- Similarity metric: normalized cross-correlation
- Reference per modality



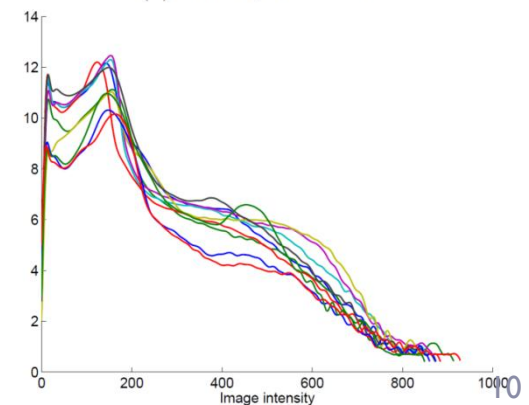
(a) 3DRA, before IIS



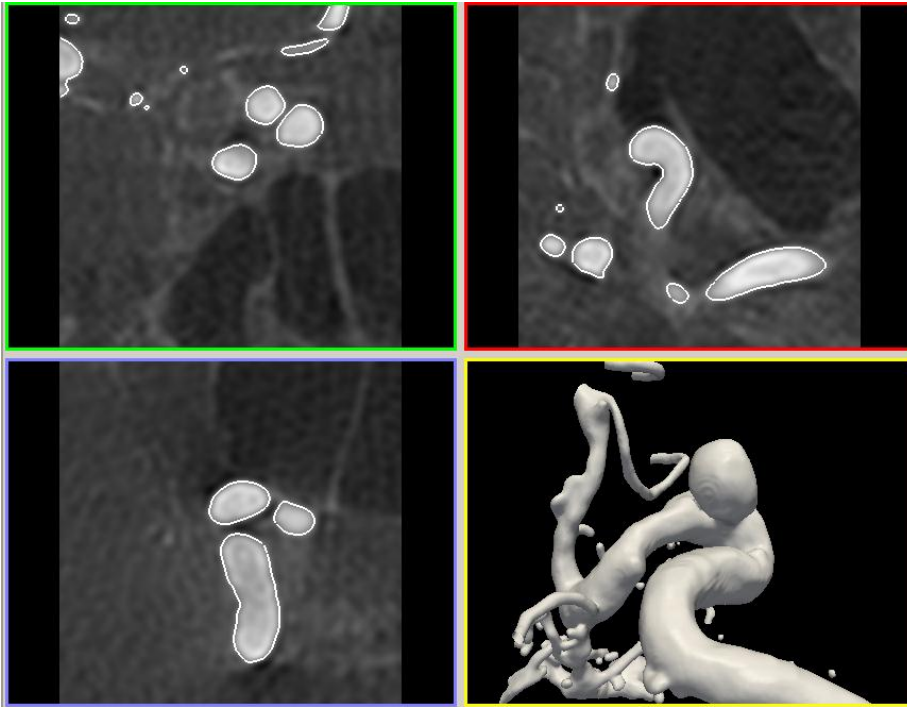
(b) MRA, before IIS



(c) 3DRA, after IIS

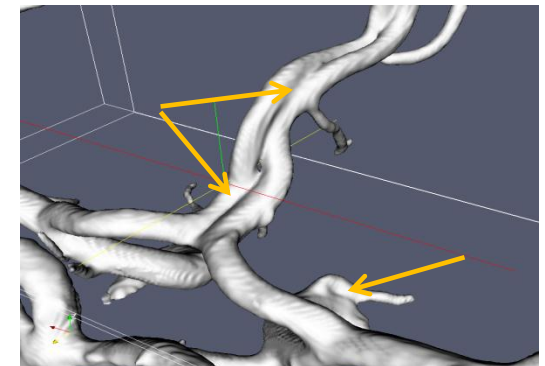
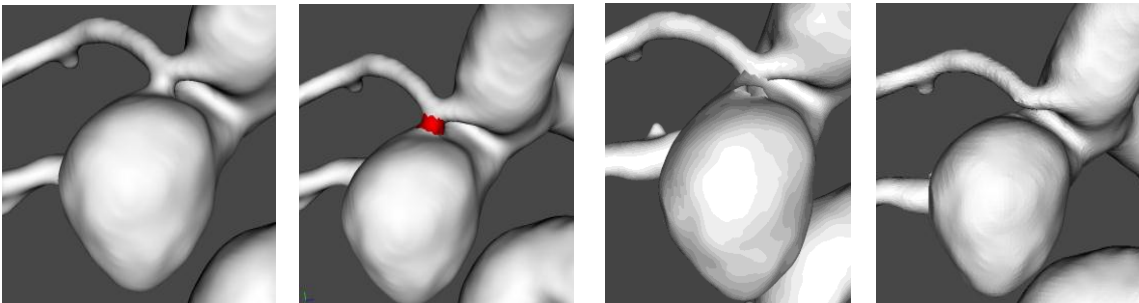


(d) MRA, after IIS

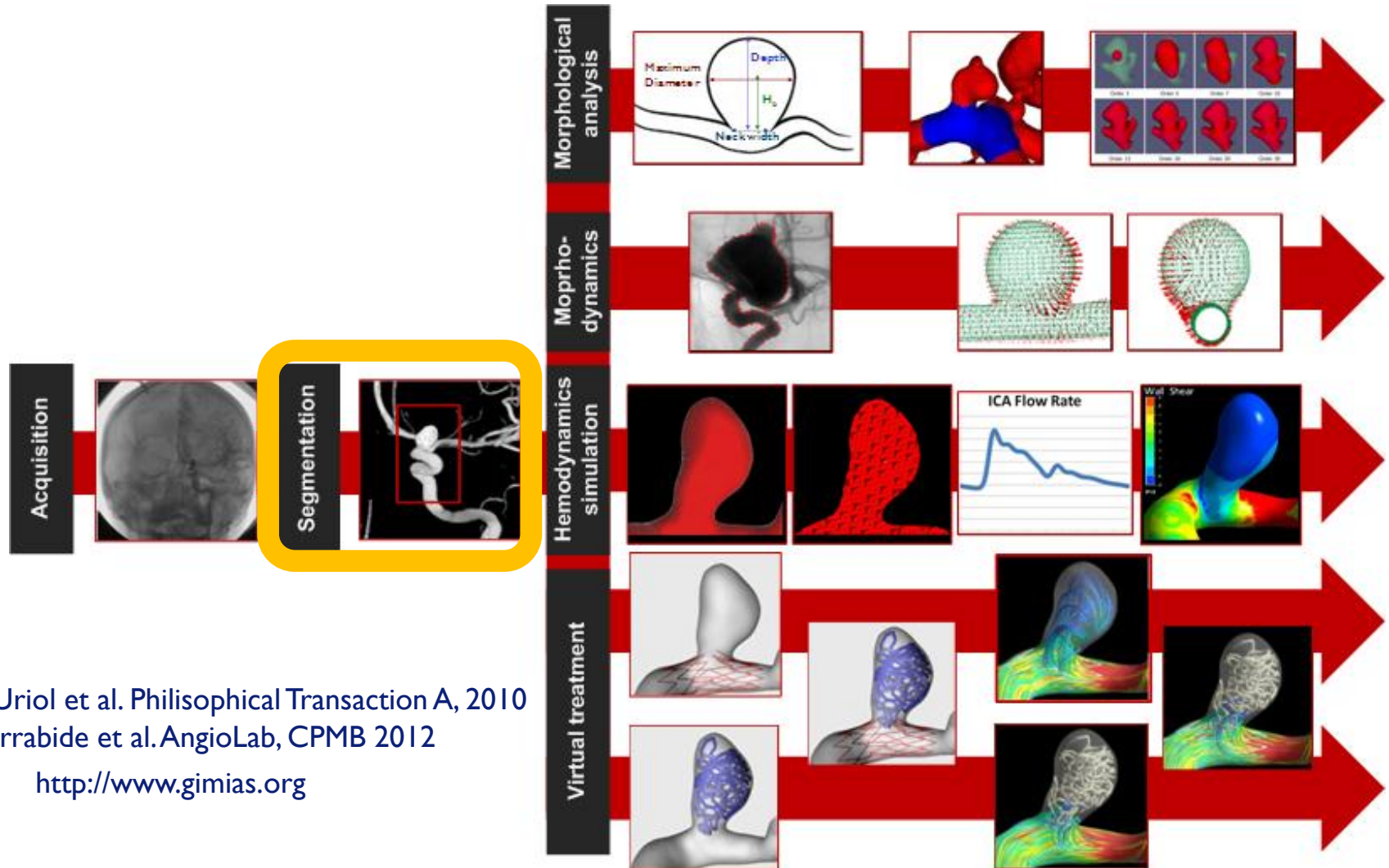


■ Difficult problem: Touching vessels

- Requires manual post-processing



Use in aneurysm management pipeline

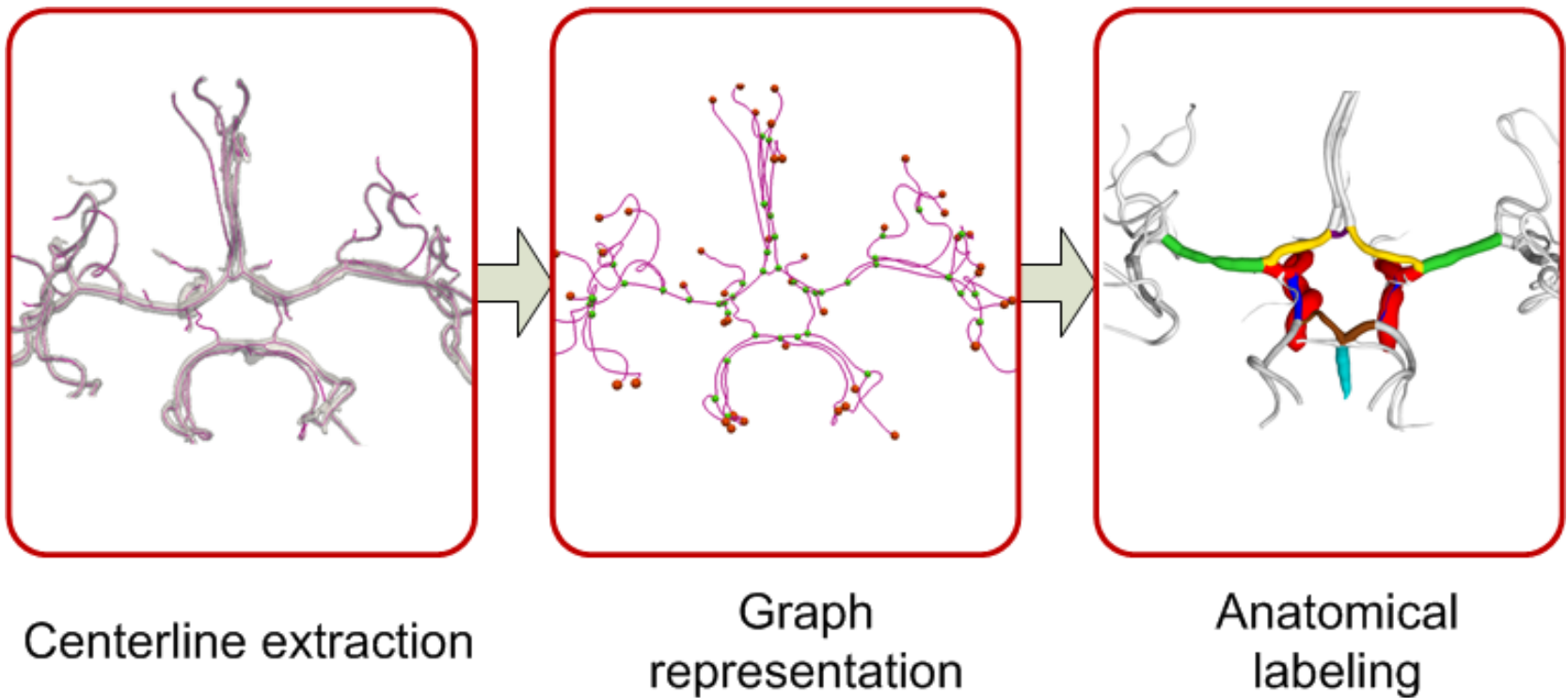


M-C.Villa-Uriol et al. Philosophical Transaction A, 2010

I. Larrabide et al. AngioLab, CPMB 2012

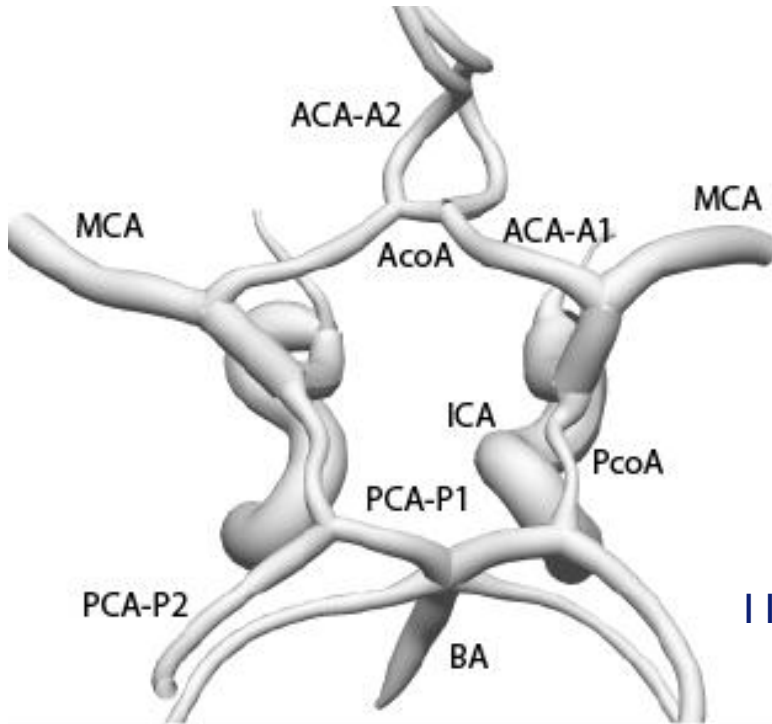
<http://www.gimias.org>

T2: ANATOMICAL LABELING OF THE CIRCLE OF WILLIS

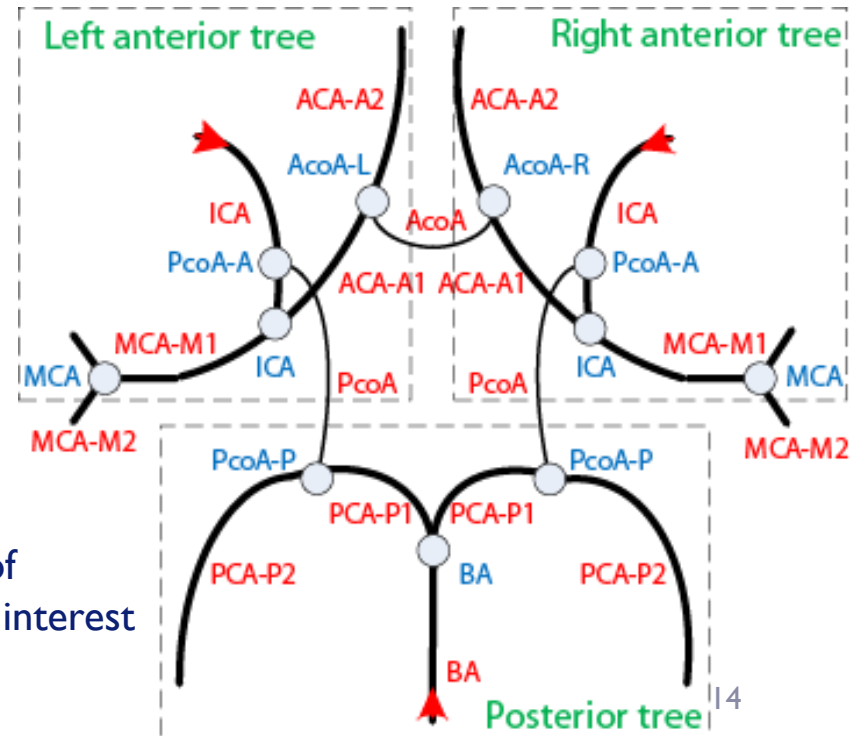


H. Bogunović, J.M. Pozo, R. Cardenes, L. San Roman, and A.F. Frangi:
Anatomical labeling of the Circle of Willis using maximum a posteriori estimation.
Under Review.

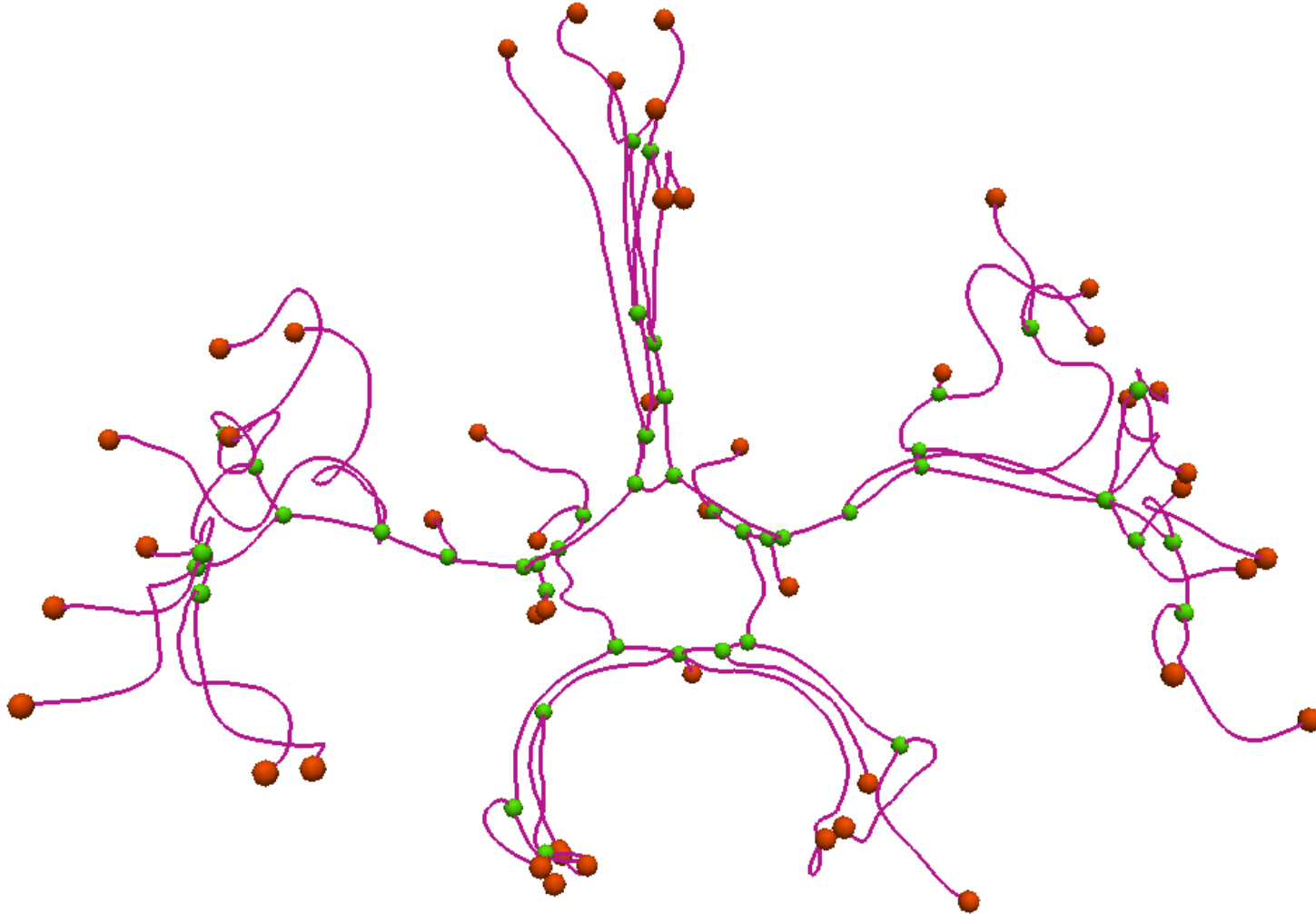
- Objective: Establish anatomical correspondence between subjects in the region of the Circle of Willis (CoW)
 - Enables subsequent geometric characterization and population analysis of the entire CoW
- Arteries form a graph containing a cycle with multiple roots
 - Unique to the CoW



Detection of
|| bifurcations of interest

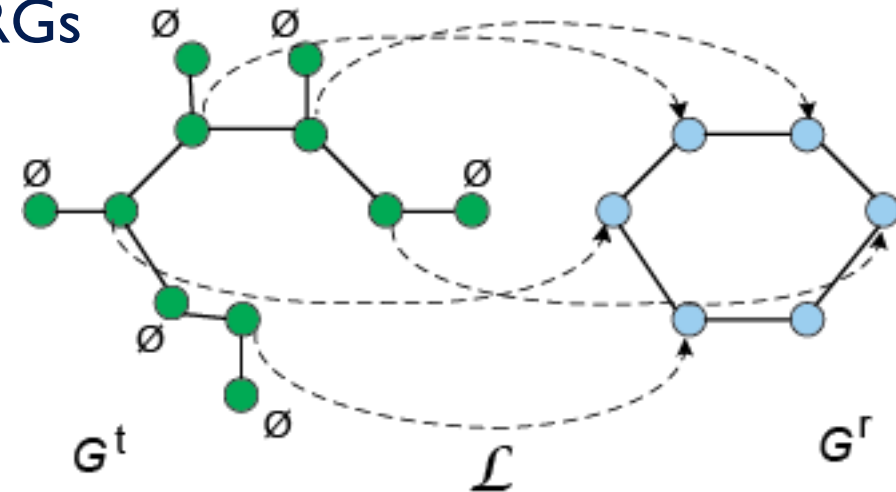


Segmentation and graph extraction



■ Labeling as mapping between ARGs

$$\mathcal{L} : V^t \rightarrow V^r \cup \{\emptyset\}$$



■ Availability of a knowledge base (KB)

- Set of reference graphs $\{V^r\}$
- Sample vertex attributes $\{A^r\}$
- Joint BoI configuration appearance $\{V^r\}$

■ Maximum a posteriori probability $\mathcal{L}^* = \arg \max_{\mathcal{L}} P(\mathcal{L} | \hat{G}^t, \text{KB})$

$$P(\mathcal{L} | G^t, A^t, R^t, \text{KB}) \propto \underbrace{p(A^t | \mathcal{L}, G^t, R^t, \text{KB})}_{\text{likelihood}} \underbrace{P(\mathcal{L} | G^t, R^t, \text{KB})}_{\text{prior}}$$

likelihood

prior

Likelihood term $p(A^t | \mathcal{L}, G^t, R^t, \text{KB})$

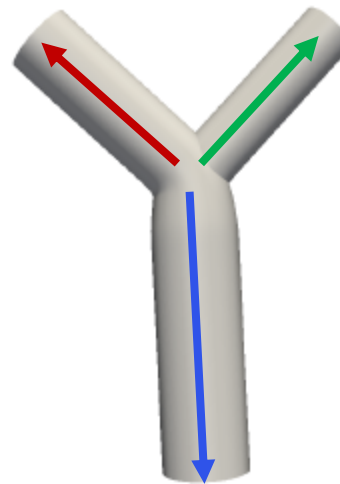
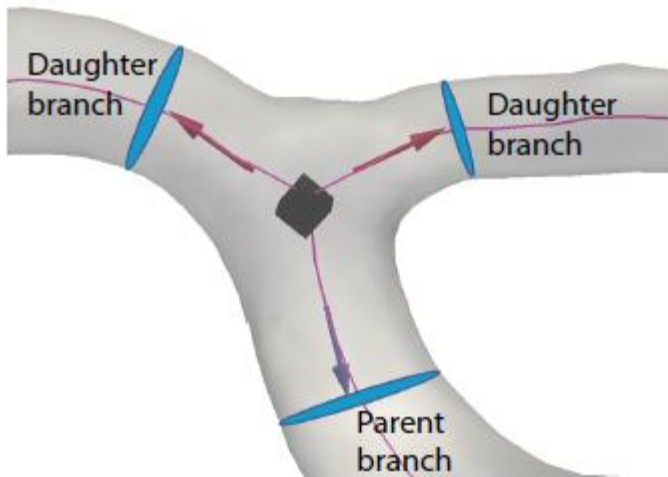
- Independency of attributes assumed

$$p(A^t | \mathcal{L}, G^t, R^t) = p(A^t | \mathcal{L}, V^t) = \prod_{i=1}^N p(a_i^t | \mathcal{L}(v_i^t))$$

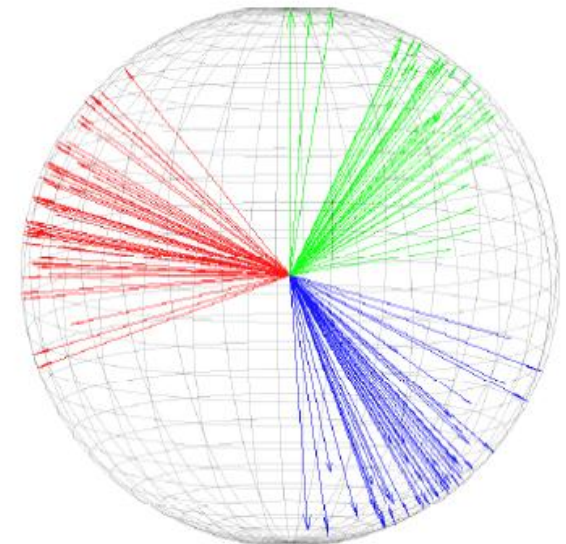
- Each bifurcation a 7-tuple.

- Element of Riemannian manifold

$$a = (\mathbf{x}, \mathbf{n}_0, r_0, \mathbf{n}_1, r_1, \mathbf{n}_2, r_2) \in \mathcal{M} = \mathbb{R}^3 \times S^2 \times \mathbb{R}^+ \times S^2 \times \mathbb{R}^+ \times S^2 \times \mathbb{R}^+$$



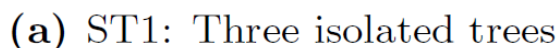
Cylindrical model



ICA terminal bifurcation
Population distribution

- Assures the labels follow the ordering of the reference graph
 - Only compatible labelings (L_c^t) allowed

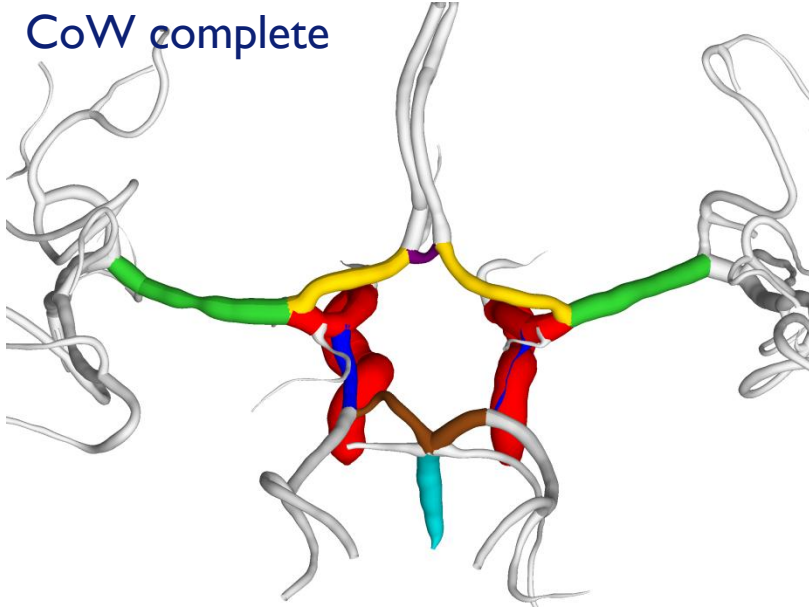
- L_c : Labelings compatible with a reference graph



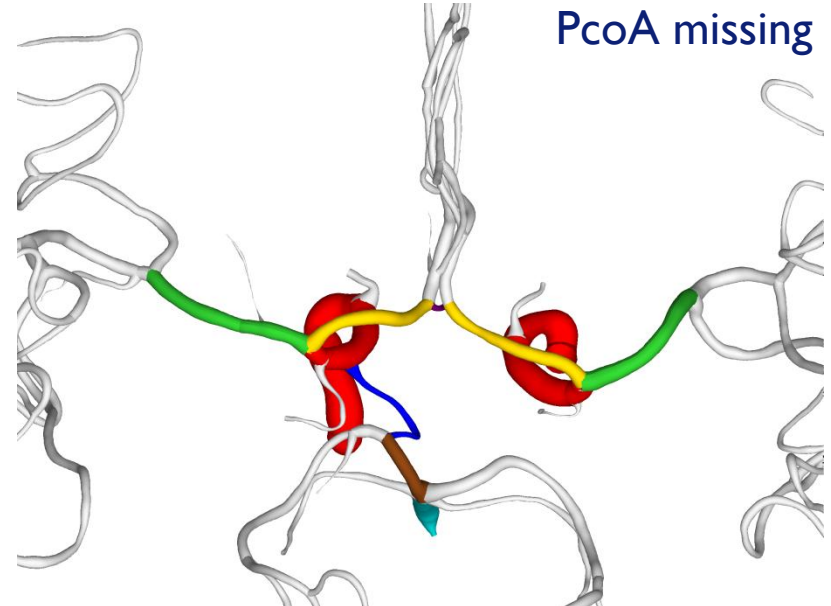
T2:Anatom. Labeling

Results

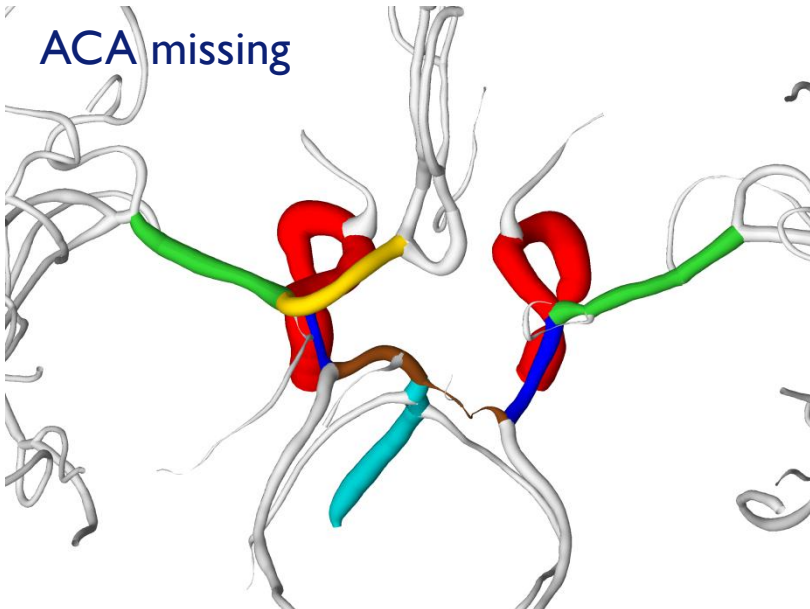
CoW complete



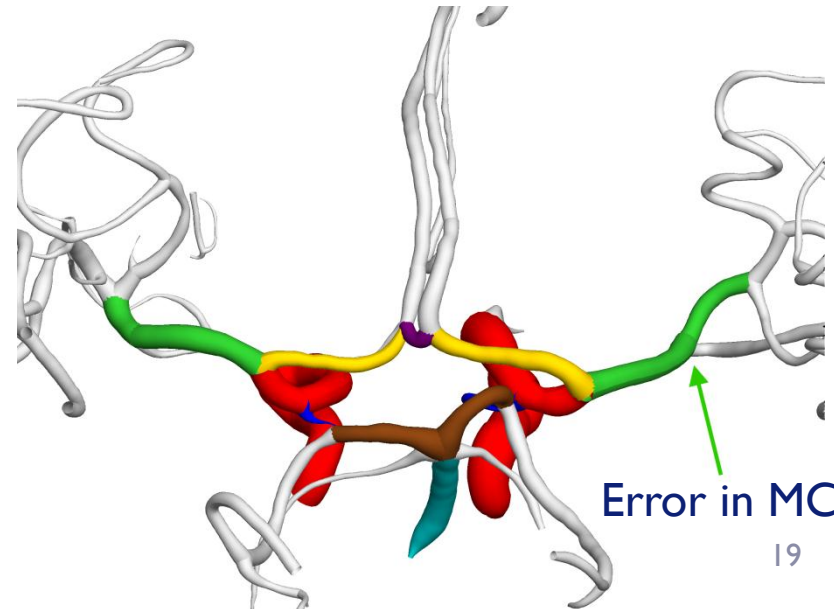
PcoA missing



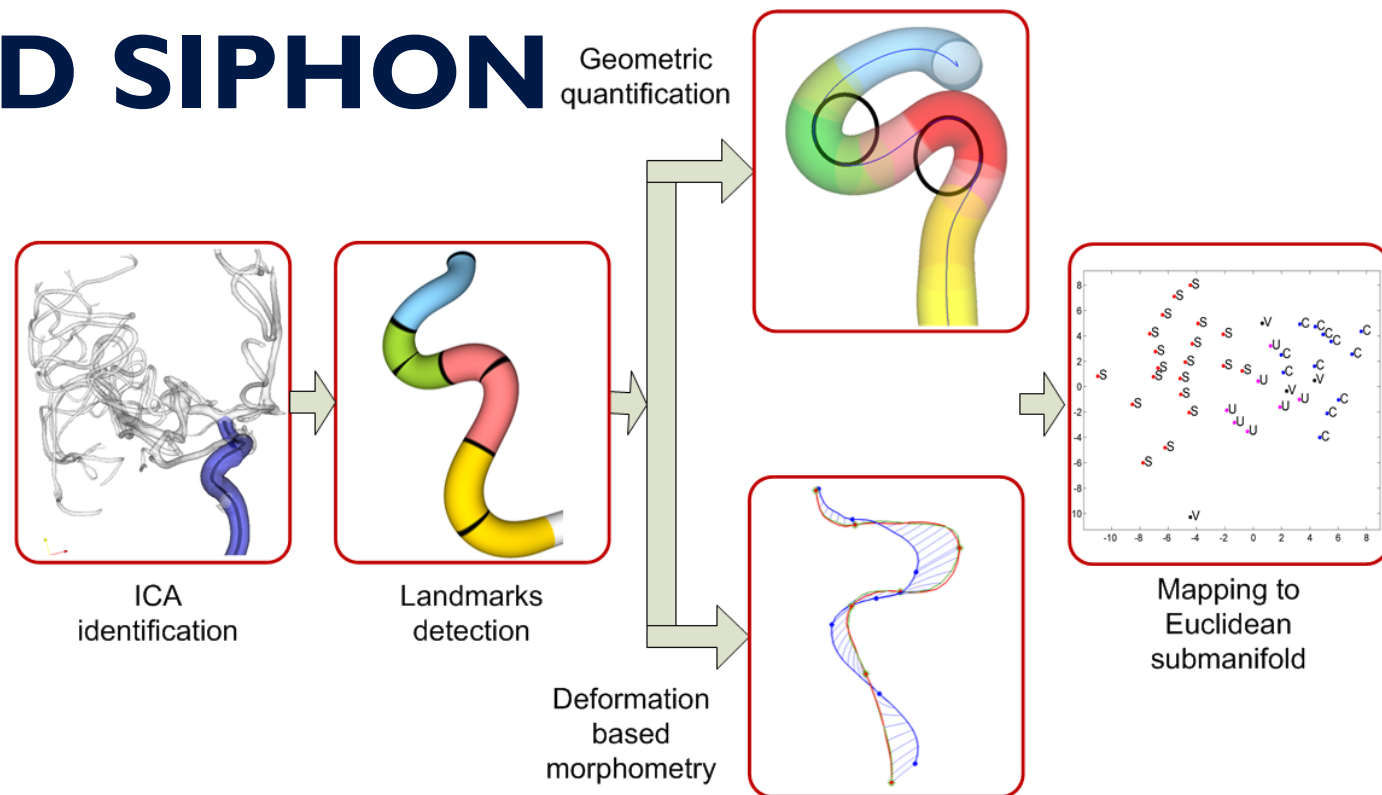
ACA missing



Error in MCA

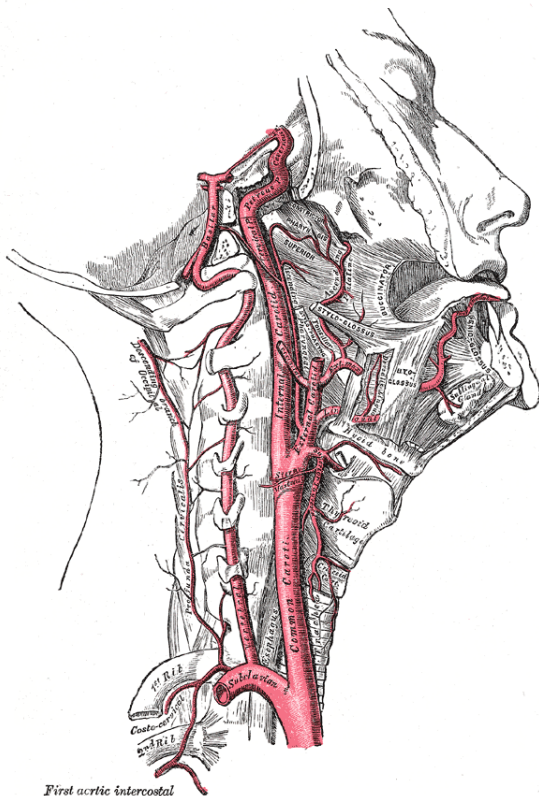


T3: GEOMETRIC CHARACTERIZATION OF THE CAROTID SIPHON



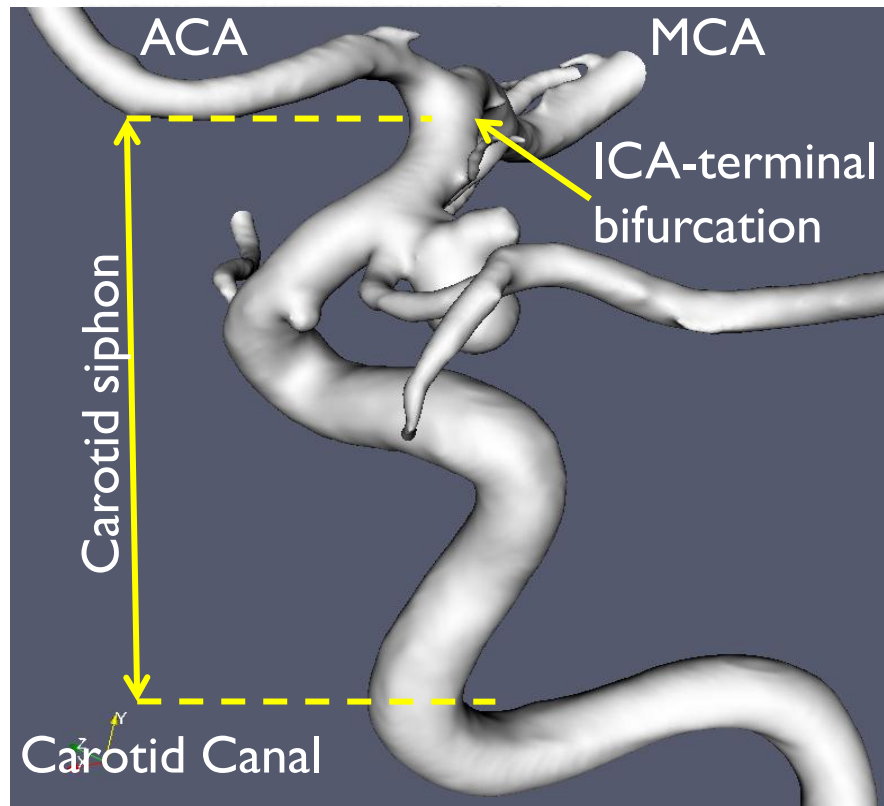
H. Bogunović, J. M. Pozo, R. Cardenes, M. C. Villa-Uriol, R. Blanc, M. Potin, and A. F. Frangi: Automated landmarking and geometric characterization of the carotid siphon. *Medical Image Analysis*, vol. 16(4), May 2012, pp. 889-903.

- Objective: Describe geometric variability of carotid siphon
 - Large geometric variability prerequisite for being a risk factors
 - 30% of aneurysms occur there
 - Important for stent fitness, endovascular accessibility



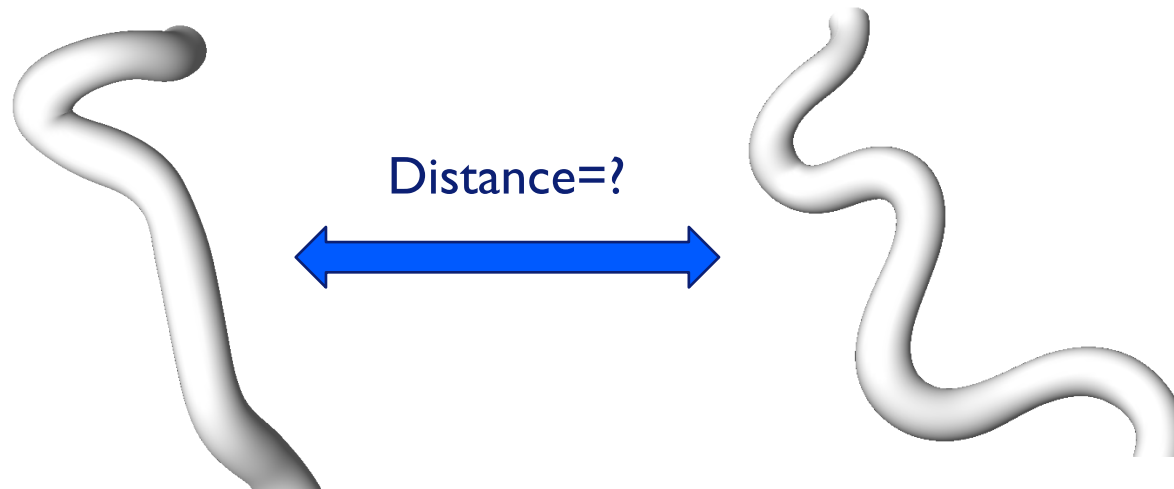
First aortic intercostal

Henry Gray's Anatomy of the Human Body



■ Carotid siphon shape space

- Finding a suitable representation and metric
- Statistical analysis



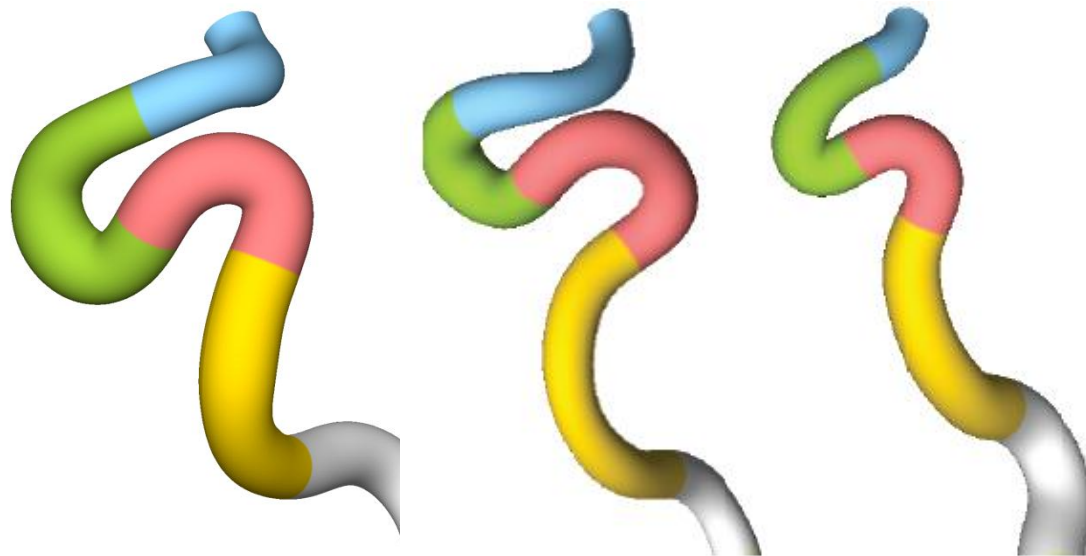
■ Option 1: Shape described as a vector of geometric features

- Principal component analysis

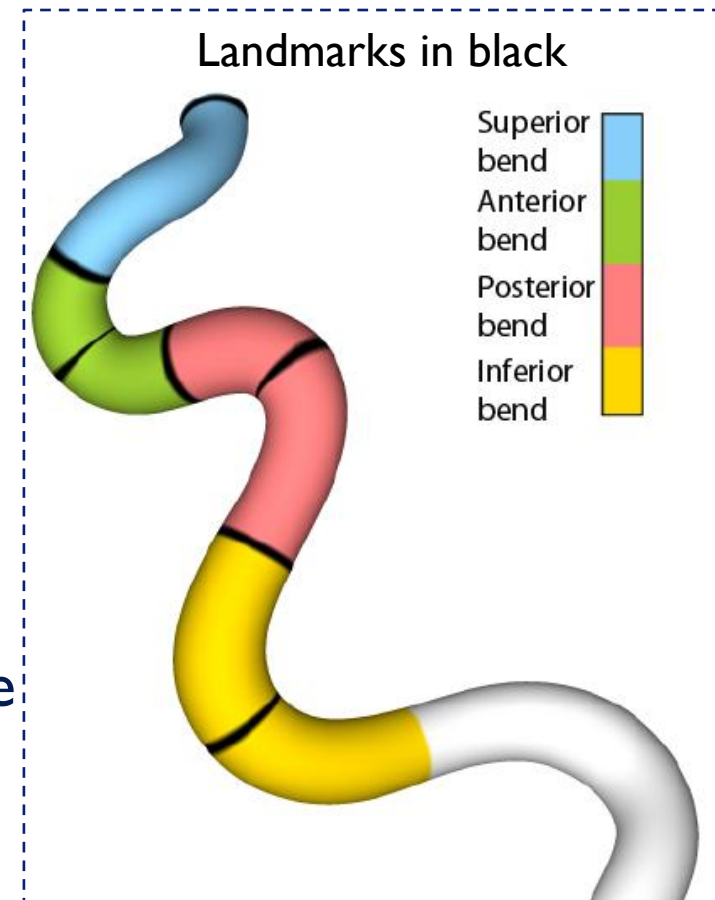
■ Option 2: Deformation based morphometry

- Pairwise distance matrix + mapping to Euclidean submanifold

Four bend model



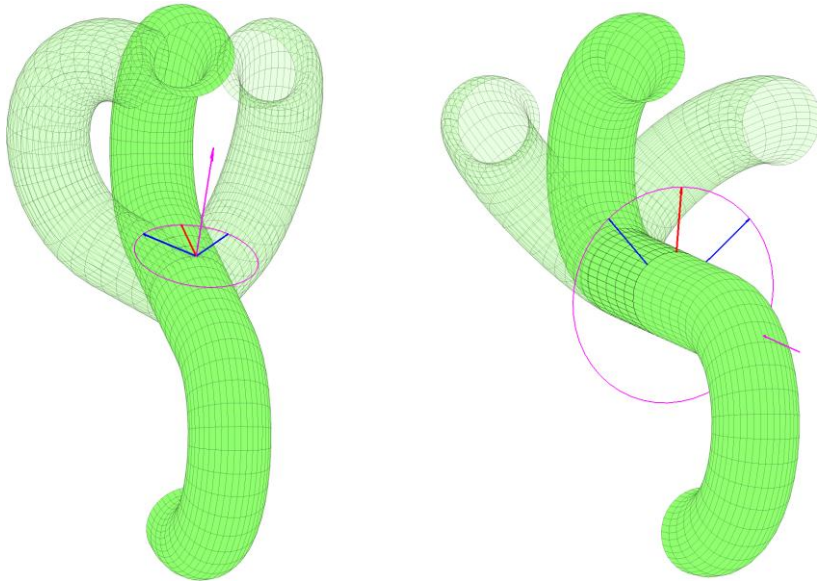
- Landmarks as points of correspondence
 - Define region of interest



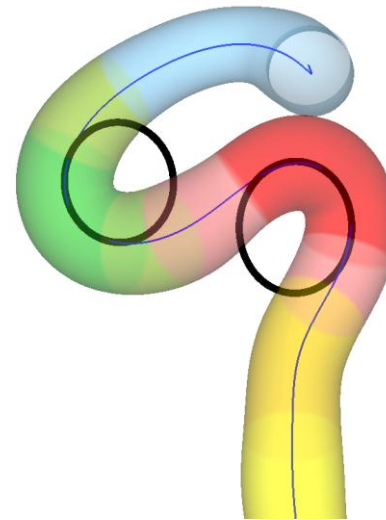
Geometric quantification

■ Geometric feature vector (scale invariant)

Change of osculating planes



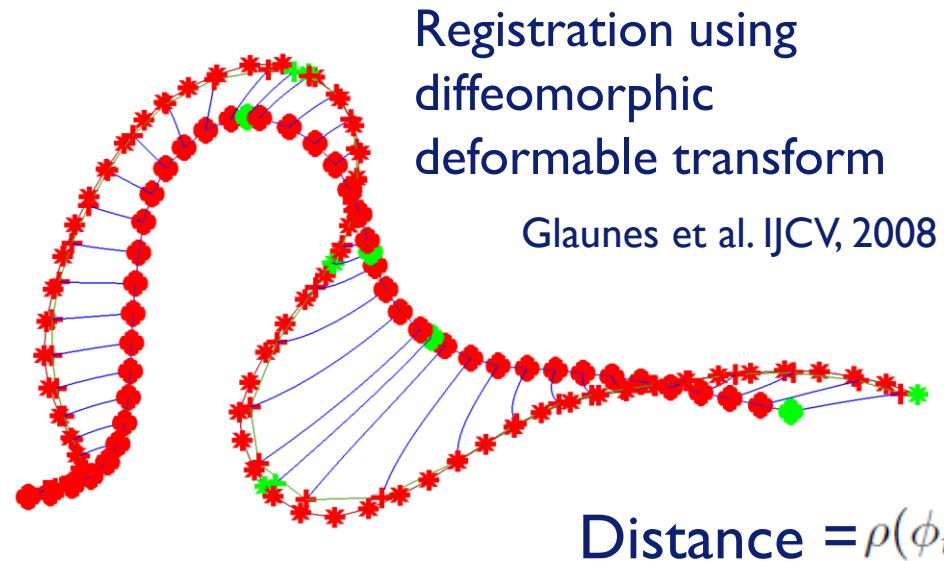
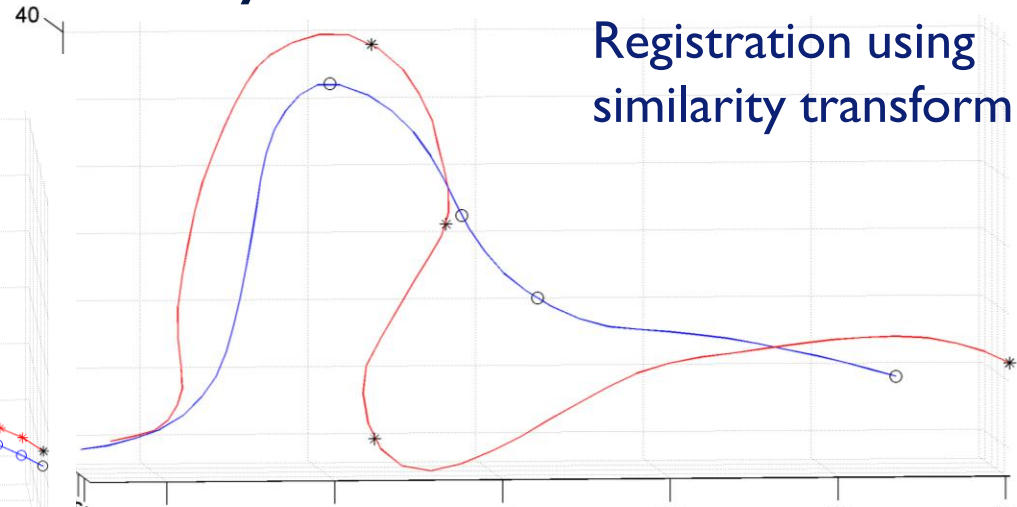
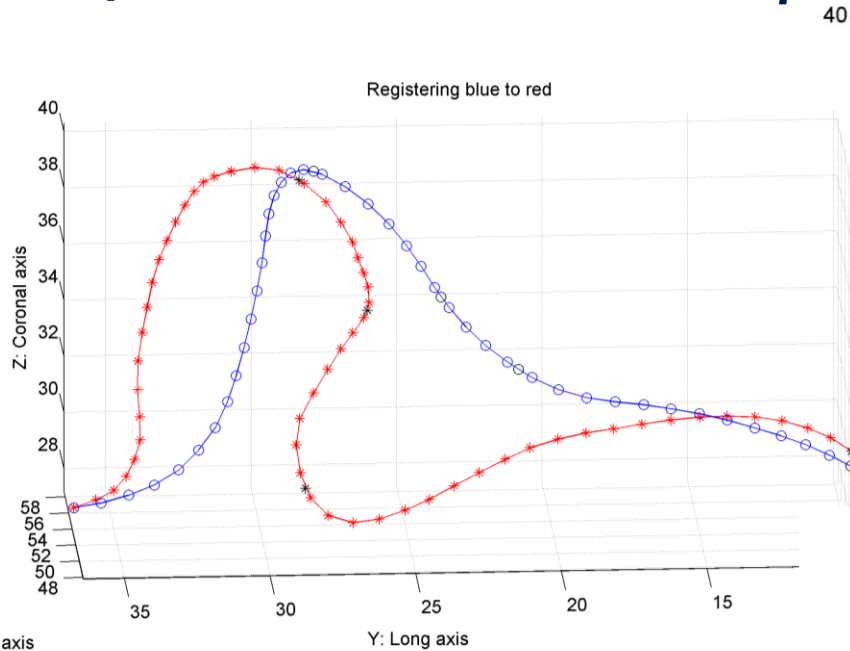
Bending radii



■ + global features

- Tortuosity
- Bending and twisting energy
- Curvature and torsion ratio

Deformation based morphometry - LDDMCM



$$J_{C,S}(\phi_t) = \gamma \rho(\phi_t)^2 + E(\phi_1(C), S)$$

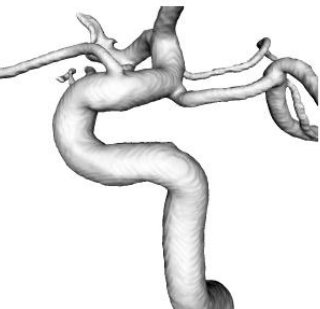
$$J_{C,S,\vec{x},\vec{y}}(\phi_t) = \gamma \rho(\phi_t)^2 + \gamma_{cr} E_{cr}(\phi_1(C), S) + \gamma_{lm} E_{lm}(\phi_1(\vec{x}), \vec{y})$$

T3: Carotid Siphon

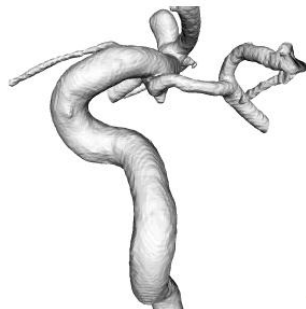
Statistical Analysis

Shape prototypes

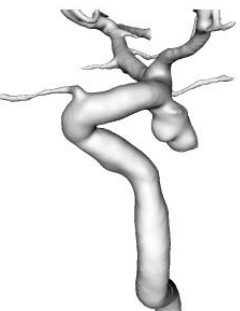
- Characterization evaluation
- Related to treatment difficulty



(a) U-type



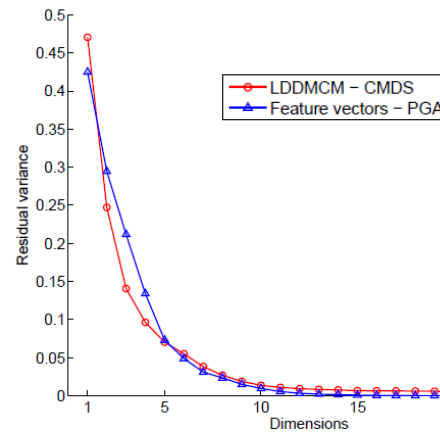
(b) C-type



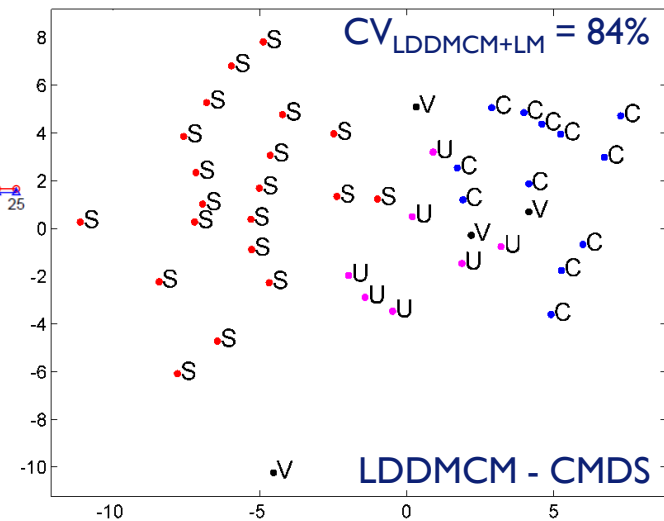
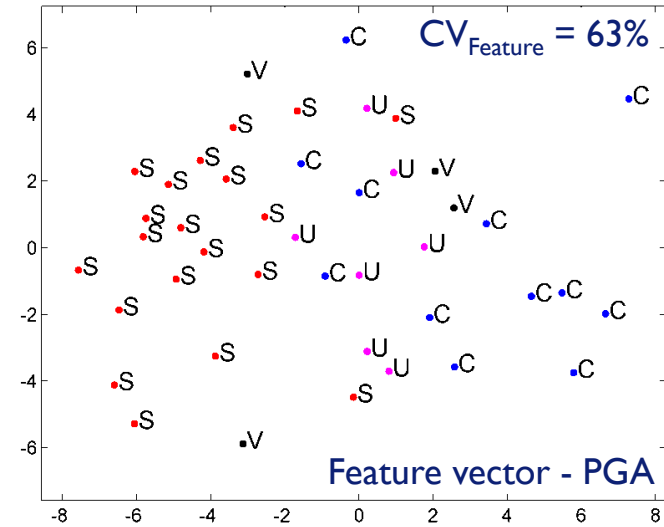
(c) V-type



(d) S-type



Embedding in 2D Euclidean space



CONCLUSIONS

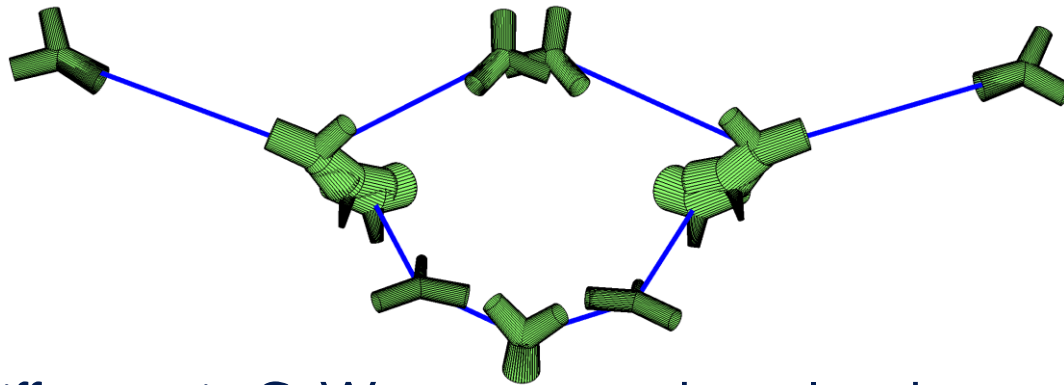
Still open problems:

- Are two vasculatures effectively the same or are they different? (pairwise statistics)
 - Finding a metric in the space of vasculatures (CoWs).
 - Measures that are closely clustered for similar vasculatures and are markedly different otherwise.
- How to model graph/tree-like structures and their variations? (groupwise statistics)
 - Atlas: mean and principal modes of variation (PCA)
 - Change of topology: Data space is strongly non-Euclidean



Start answering questions:

- How does the average CoW look like and what are its principal variations?



- Is there any difference in CoW geometry and topology between men and women?
 - Prevalence of aneurysms is larger in women, could it be due to different CoW geometry between them?
- Is the difference in handedness reflected in the CoW?
- Does the CoW change with aging and how?
- What would be considered normal variability of the CoW and what would be deviations associated with the risk of developing a pathology?
- Can we predict or estimate a risk of aneurysm rupture, from the CoW?

Acknowledgments

Sources of funding



Agència
de Gestió d'Ajuts
Universitaris
i de Recerca



Generalitat
de Catalunya

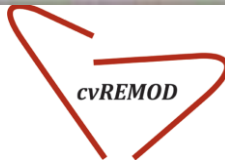
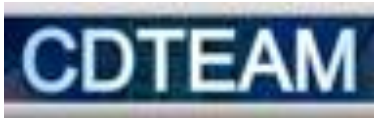


aneurIST
Integrated biomedical informatics for the management of cerebral aneurysms



Unión Europea

Fondo Europeo de
Desarrollo Regional



GOBIERNO
DE ESPAÑA

MINISTERIO
DE CIENCIA
E INNOVACIÓN

PHILIPS

sense and simplicity

Acknowledgments

People

CISTIB Center for Computational
Imaging & Simulation
Technologies in Biomedicine



<http://www.cistib.upf.edu/>